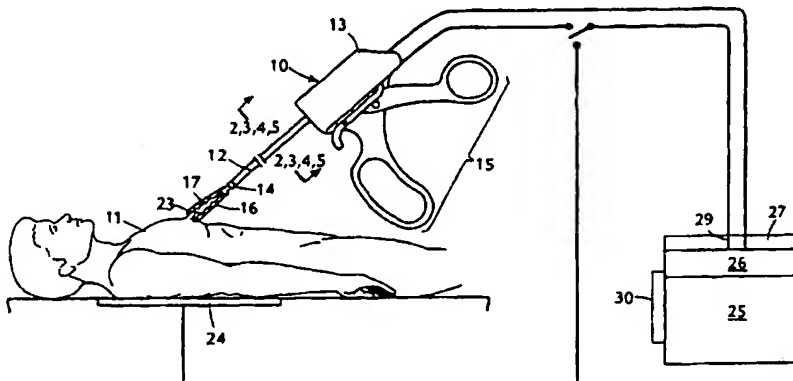


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(54) Title: VASCULAR TISSUE SEALING PRESSURE CONTROL AND METHOD



(57) Abstract

A clamping force mechanism (10) and its method of use with electrosurgery allow a user to seal and/or joint patient's particular vascular tissue; the mechanism is elongate with user and patient ends (14). An actuator (15) is at the user end (13) and the effectors are at the patient end (14). Each effector has a face of an area to contact the particular vascular tissue. A lost motion connection (18) transfers user actuation to the effectors to hold a predetermined clamping force during electrosurgical tissue sealing. A yielding member (19) in the lost motion connection clamps the particular tissue between the faces with a predetermined force. The yielding member (19) is a spring (20), slip clutch (36) or hydraulic coupling possibly near the actuator (15). An active electrode is carried on one end effector and a return electrode (24) contacts the tissue so an electrosurgical energy supply (25) connected thereacross delivers energy therebetween. A feedback circuit (27) responds to parameters of energy delivered to tissue. A temperature sensor (28) on one face and an impedance monitor (29) respond to energy delivered. A control (30) applies energy to held tissue to seal and/or join it. The method transfers user actuation of the effectors with the lost motion connection (18), maintains clamping force while sealing and applying electrosurgical energy to seal and/or join held tissue. Energy is applied to a temperature or an impedance. The method shifts the yielding member (19) so the opposing faces (17) clamp the particular tissue therebetween with the force from the spring (20), via a transfer rod or by the hydraulic coupling or the slip clutch (36) for a range of pressure.

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5 VASCULAR TISSUE SEALING PRESSURE CONTROL AND METHOD

1. Field of the Invention A clamping force mechanism for an instrument
10 allows a user to apply force within an preferred range to hold particular vascular
tissue of a patient during application of electrosurgical energy to seal and /or join the
particular tissue.

2. Background of the Disclosure Sealing and/or joining of particular
vascular tissue during surgery is an essential part of an operation or procedure.
15 Sutures, staples and adhesives have been used with varying levels of success.
These prior techniques and the material and equipment used fail to minimize or limit
the damage to the particular tissue and most importantly do not eliminate foreign
body reactions of the patient to the added material. Specifically, the reaction of the
patient's body is normally to surround the foreign body, i.e. added scar tissue, with
20 barrier cells to thereby isolate the foreign matter from the normal cells within the
patient. Consequently, the scar or evidence of the trauma is increased in size. The
added material increases the cost of any surgical operation or procedure and post
surgical concerns and healing.

Vascular tissue sealing and/or joining is important to the minimization of
25 and/or elimination of bleeding or to the reconnection of tissue structures after
surgical removal of undesirable organs or growths. Electrosurgery has been used to
cut and coagulate tissue but the control needed to cleanly seal and /or join cut tissue
and coagulate the bleeders has been lacking particularly in highly vascularized tissue,
i.e. the particular patient tissue of interest and concern herein. Specifically, various
30 approaches to coagulation, fulguration, cauterization for forming minimal and or
flexible eschar over the bleeders have been tried. Different high frequency
waveforms for coagulation by electrosurgical energy, argon gas enhanced
coagulation and non sticking electrosurgical electrodes have been designed
manufactured and sold with varying degrees of success at reducing healing time and
35 the amount of evidence of surgical intrusion. All of the foregoing increases cost and
complexity of surgical healing.

U.S. Patent 4,043,342 has electrosurgical implements with sesquipolar
electrode structures with active and return electrodes supported by insulated

5 connectors respectively spring biased.

WO 9313719 has an electrosurgical instrument including a support structure with two electrodes interconnected with it to allow relative motion there between. A biasing device, such as a spring, urges the current return electrode into contact with tissue when the active electrode is positioned for surgery. The return electrode
10 is longitudinally and laterally movable relative to the active electrode. A signal source provides a tissue cutting signal and a coagulation signal. The current return electrode has a tissue contact surface which defines a planar interface with the tissue during surgery. The active electrode is transversely movable relative to the interface. It increases contact surface to reduce likelihood of tissue damage and to
15 easily control cutting depth. U.S. Patent 5,047,027 has a bipolar electrosurgical instrument designed for resecting tumorous growths from the esophagus bladder or other internal organ wherein the site of the tumor is reached by way of an endoscope. The cutter is dimensioned to fit down the central lumen of the endoscope. An elongated flexible tube has a conductive helical spring cantilevered
20 from the distal end of the tube, forming a return electrode and conductive wire hoop spaced a predetermined gap distance from the distalmost convolution of the helical spring and whose plane is perpendicular to the longitudinal axis of the flexible tube forms the active electrode.

Wires for applying a high frequency RF voltage across the electrodes extend
25 through the lumen of the flexible tube. As the distal end portion of the instrument is dragged over the tumor to be resected, the cantilevered helical spring is laterally displaced, allowing the RF current leaving the active hoop electrode to cut through the tumorous tissue.

U.S. Patent 5,007,908 has an instrument with an elongate flexible tubular
30 member having a proximal end, a distal end and multiple lumens extending between them. Affixed to the distal end of the tube is a bullet-shaped ceramic tip member having a centrally-disposed longitudinal bore passing through the side wall of the tip member. The ceramic exterior surface of the tip member is covered with a conductive layer forming a first inactive electrode. An electrical conductor joined to
35 that electrode surface feeds back through a lumen of the tube to its proximal end where it may be coupled to an electrosurgical generator. Also running a through a lumen in the tube is another conductor which can be made to project outwardly

5 through the opening in the top member. A hub having a spring-loaded plunger is affixed to the proximal end of the tube with the plunger joined to the wire so that when the plunger is depressed the distal end of the wire will project a short distance beyond the extremity of the tip member. By coupling this second conductor to an electrosurgical generator, it becomes the active electrode of a bipolar pair.

10 U.S. Patent 5,290,286 has an electrosurgical instrument with a bipolar pair of conductive electrodes for the cutting of tissue in which at least one electrode is moveable in relation to the other. The electrodes are mounted relative to an insulating plug, which is secured at the distal end of a tubular member. Pressure exerted on a thumb loop shifts the position of one electrode relative to the other.
15 Upon application of RF voltage, the distance at which the electrodes are placed controls the amount of arcing which will occur between electrodes, when placed within a proper range. The electrodes are supplied with power from a standard RF energy source, controlled from a foot or hand switch. The insulating plug may further include metal traces disposed on the peripheral surface. When energized, these
20 traces function as a bipolar pair of electrodes for effecting electrocoagulation of tissue and blood. The instrument is for insertion in laparoscopic trocar or endoscope for trimming small polyps from wall of colon and removal of tissue, and coagulating particular vascular tissue areas.

U.S. Patent 5,342,357 has a cauterization system with a radio frequency
25 energy source including a control unit connected to the energy source, and an electrosurgical probe. The probe has a handle with an elongate member extending from the handle. The distal end of the elongate member is tapered and includes a cauterization tip and a retractable cutting electrode. The probe includes a conduit for the transmission of cooling fluid to the distal end. The temperature of the
30 electrode on the distal end of the probe is monitored and is used to control the rate of flow of the cooling fluid to the tip. A generator supplies electrical energy to the electrodes and the impedance of the tissue between the electrode is monitored to prevent tissue damage due to high temperatures. The system controls transfer of heat to tissue during surgery and prevents tissue or coagulant from welding to
35 energy delivering electrode.

None of the aforementioned equipment has offered the surgeon the level of control needed to remodel and reform the tissue with electrosurgical energy. No

5 mechanism for the application of clamping pressure, electrosurgical energy and temperature to seal and/or join vascularized tissue has been found. The tissue of the patient includes collagen which has been found to bind an injury or wound, surgical or otherwise, when subject to adequate pressure and temperature. Collagen can be melted and resolidified into a load resistant natural tissue coagulant so the reformed
10 structure is capable of enduring loads similar to that carried by uncut tissue. No mechanism for the adequate and proper application of temperature and pressure is known.

A related patent application entitled "Energy Delivery System for Vessel Sealing", attorney docket number PC 9202, has been filed concurrently with this
15 application.

SUMMARY OF THE INVENTION

A clamping force mechanism for a clamping electrosurgical instrument allows a user to seal and/or join particular vascular tissue of a patient. The clamping force
20 mechanism is preferably elongate having user and a patient ends. An actuator may be at the user end and a pair of the end effectors might be at the patient end so the pair of end effectors when connected to the actuator operate from the user end to control the motion of the end effectors. The pair of end effectors may each have an opposing face of an area for contact with the particular vascular tissue of the
25 patient.

A lost motion connection is most preferably in the preferred embodiment between the end effectors and the actuator to transfer user manipulation of the actuator to the end effectors and for maintaining predetermined clamping force applications during journey and/or sealing the particular vascular tissue of the patient.
30 A yielding member may be included in the lost motion connection so the opposing faces clamp the particular tissue of the patient therebetween with force from the yielding member. The yielding member may in the preferred embodiment include a spring located near the actuator at the user end.

An elongated transfer rod in the lost motion connection is preferably between
35 the spring near the actuator and the end effectors at the patient end for movement thereof between an open position for receiving the particular tissue of the patient to a clamping position for maintaining the predetermined force on the particular tissue

5 of the patient between the end effectors. A locking linkage coupled to the actuator and the yielding member may retain the opposing faces held against the particular tissue of the patient therebetween with the force from the yielding member to achieve the predetermined force. Stepped latching positions on the actuator preferably permit the user to selectively set the locking linkage and the yielding
10 member establishing different levels of force for the particular vascular tissue sealed to retain the set force in accord with the particular tissue being sealed. The stepped latching positions may be associated with different particular vascular tissue such as arteries or veins or mesentary.

An active electrode is most preferably carried on one of the end effectors.
15 A return electrode can also contact the tissue of the patient. An electrosurgical energy supply connects across the active electrode and the return electrode to deliver electrosurgical energy between and across the active electrode and the return electrode when the particular tissue of the patient is held by the end effectors. The electrosurgical energy supply may include an electrosurgical generator.

20 A feedback circuit can be in the electrosurgical generator and in circuit with the active and the return electrodes to respond to parameters indicative of energy delivery through the particular vascular tissue of the patient interposed between the active and return electrodes.

A temperature sensor may also be in the feedback circuit and preferably
25 carried on one of the opposed faces; the sensor to respond to the temperature of the particular vascular tissue of the patient between the opposed faces during delivery of electrosurgical energy. An impedance monitor in the feedback circuit can also be electrically hooked up to the electrosurgical generator to respond to the impedance changes of the particular vascular tissue of the patient between the active and return
30 electrode during delivery of electrosurgical energy.

A control associated with the electrosurgical energy supply most preferably applies electrosurgical energy to the held particular tissue of the patient in response to the application of the predetermined force for the sealing the particular tissue between the end effectors.

35 Alternatively, in a bipolar circuit the return electrode could be on one of the pair of end effectors opposite the active electrode. Optionally, the return electrode might be on one of the pair of end effectors that carries the active electrode with an

5 electrical insulator disposed between those active and the return electrodes. Similarly, the return electrode may be a pad connected to the tissue of the patient and this is a monopolar circuit.

The yielding member might be a hydraulic coupling as part of the lost motion connection between the end effectors. The hydraulic coupling can be located near
10 the actuator. The yielding member could be a slip clutch within the lost motion connection near the actuator at the user end.

The pair of end effectors may have opposing faces each of an equal and preset area to clamp the particular tissue of the patient therebetween with the force from the yielding member so that a force is applied to the particular tissue in a
15 preferred range.

A method allows a user to clamp and apply force and electrosurgical energy to seal and/or join particular vascular tissue of a patient with the clamping force mechanism for the instrument. The steps of the method may include transferring user manipulation of the actuator to the pair of end effectors with the lost motion
20 connection, maintaining with the lost motion connection predetermined clamping force application during sealing of the particular tissue between the end effectors and applying electrosurgical energy for sealing the held particular tissue of the patient in response to the clamping thereof between the end effectors with a control associated with the electrosurgical energy supply.

25 The method step of applying electrosurgical energy can include responding to the parameter of the temperature of the particular tissue of the patient between the end effectors during delivery of electrosurgical energy with the feedback circuit including the temperature sensor carried on one of the opposed faces.

The method step of applying electrosurgical energy may be limited by the
30 impedance of the particular tissue of the patient between the active and return electrodes during delivery of electrosurgical energy with the impedance monitor.

The method step of maintaining the predetermined clamping force during sealing of the particular tissue may be performed by shifting the yielding member so the opposing faces clamp the particular tissue of the patient therebetween with force
35 from the yielding member.

The method step of shifting preferably secures the predetermined clamping force during sealing of the particular tissue by the resilient bias from the yielding

5 member and by most preferably including the step of urging with the spring.

The method step of shifting could alternately secure the predetermined clamping force during sealing of the particular tissue by the yielding member with the step of moving the end effectors between their open position for receiving the particular tissue to the clamping position with the elongated transfer rod.

10 The method step of shifting with the actuator may secure the predetermined clamping force during sealing of the particular tissue of the patient by the resilient bias of the yielding member with the alternative step of urging with the hydraulic coupling.

The method step of shifting with the actuator can secure the predetermined
15 clamping force during sealing of the particular tissue by the resilient bias of the yielding member with the step of urging with the slip clutch.

The method step of maintaining the predetermined clamping pressure during sealing particular tissue with the step of using the force from the yielding member so that pressures within a preferred range may be achieved with the locking linkage.

5

BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1 is a schematic view of an electrosurgical supply and circuit for a clamping force mechanism to allow a user to apply force within an preferred range to hold particular vascular tissue of a patient during application of electrosurgical
10 energy to seal and /or join the particular vascular tissue.

Figure 2 is a side view in partial cross section taken along lines 2-2 of Figure 1 and showing the clamping force mechanism wherein a spring is used as a lost motion connection between the user and end effectors shown herein in a fully open position.

15 Figure 3 is a side view in partial cross section taken along lines 3-3 of Figure 1 and showing the clamping force mechanism wherein the end effectors are shown in closed position.

Figure 4 is a side view in partial cross section taken along lines 4-4 of Figure 1 and showing the clamping force mechanism wherein the end effectors are in
20 partially compressed position.

Figure 5 is a side view in partial cross section taken along lines 5-5 of Figure 1 and showing the clamping force mechanism wherein the end effectors are in the fully closed compressed position.
actuator and the pair of end effectors.

25 Figure 6 is a partial schematic view of the hydraulic coupling for the lost motion connection.

Figure 7 is a partial schematic view of the slip clutch for the lost motion connection.

DETAILED DESCRIPTION OF THE INVENTION

30 A clamping force mechanism 10 of an instrument allows a user to clamp and apply force and electrosurgical energy to seal and /or join particular vascular tissue of a patient 11, in Figure 1. The clamping force mechanism 10 includes an elongate support 12 particularly good for endoscopic procedures having a user end 13 and a patient end 14. An actuator 15 is at the user end 13 or operation by the user. A
35 pair of the end effectors 16 is at the patient end 14 and the pair of end effectors 16 connect to the actuator 15 for operation thereby and from the user end 13 to control the motion of the pair of end effectors 16. The pair of end effectors 16 each have

5 an opposing face 17 of an area for contact with the particular tissue of the patient 11 as shown in Figures 2, 3, 4 and 5.

A lost motion connection 18 is positioned between the pair of end effectors 16 at the patient end 14 and the actuator 15 at the user end 13, in Figures 2, 3, 4 and 5. The lost motion connection 18 transfers user manipulation of the actuator 10 15 to the pair of end effectors 16 for maintaining a predetermined clamping force application during sealing the particular tissue of the patient 11 between the pair of end effectors 16. A yielding member 19 is in the lost motion connection 18 so the opposing faces 17 clamp the particular vascular tissue of the patient 11 therebetween with force from the yielding member 19. The yielding member 19 15 includes a spring 20, as part of the lost motion connection 19, between the pair of end effectors 16 at the patient end 14 and the actuator 15 at the user end 13. The spring 20 is located near the actuator 15 at the user end 13.

An elongated transfer rod 21 connected to the lost motion connection 18 is located between the spring 20 near the actuator 15 and the pair of end effectors 16 20 at the patient end 14, in Figures 2, 3, 4 and 5. The rod 21 couples to the pair of end effectors 16 for movement thereof between an open position in Figure 2 for receiving the particular tissue of the patient 11 to a clamping position for maintaining the predetermined force on the particular tissue of the patient 11 between the pair of the end effectors 16.

25 In Figures 2, 3, 4 and 5, a locking linkage 22 coupled to the actuator 15 and the yielding member 19 retains the opposing faces 17 held against the particular tissue of the patient 11 therebetween with the force from the yielding member 19 to achieve predetermined forces of compression. Figures 3, 4 and 5 show different levels of compression, i.e. no force, partial compression and full compression. This 30 is achieved with the catch 22a and notches 22b as shown but any form of stepped latching arrangement that would hold the actuator 15 in a preset position is acceptable. Stepped latching positions on the actuator 15 permit the user to selectively set the locking linkage 22 and the yielding member 19 establishing the force for the particular vascular tissue sealed to retain the predetermined force in 35 accord with the particular vascular tissue being sealed. The stepped latching positions may be associated with different particular vascular tissue such as arteries or veins or mesentary if desired. For example, arteries will require a greater closure

5 force than veins. It has been found that a closure force of greater than 1500 grams is effective for sealing arteries. A closure force of less than 500 grams is effective for sealing veins.

An active electrode 23 is carried on one of the pair of end effectors 16 in Figure 1 but could be both of the end effectors 16. A return electrode 24 is in
10 contact with the tissue of the patient 11. An electrosurgical energy supply 25 connects across the active electrode 23 of the pair of end effectors 16 and the return electrode 24. The electrosurgical energy supply 25 delivers electrosurgery between and across the active electrode 23 and the return electrode 24 when the particular tissue of the patient 11 is held by the pair of end effectors 16. The
15 electrosurgical energy supply 25 includes an electrosurgical generator 26.

A feedback circuit 27 is in the electrosurgical generator 26. The feedback circuit 27 is in circuit with the active electrode 23 and the return electrode 24 and is responsive to the parameters indicative of energy delivery through the particular tissue of the patient 11 interposed between the active electrode 23 and the return
20 electrode 24.

A temperature sensor 28 in Figure 2 is connected to the feedback circuit 27 is carried on one of the opposed faces 17 and responds to the parameter of temperature of the particular tissue of the patient 11 between the pair of end effectors 16 during delivery of electrosurgical energy. An impedance monitor 29 in
25 the feedback circuit 27 is electrically hooked up to the electrosurgical generator 26. The impedance monitor 29 responds to the parameter of the impedance of the particular tissue of the patient 11 between the active electrode 23 and return electrode 24 during delivery of electrosurgical energy.

A control 30 in Figure 1 associated with the electrosurgical energy supply 25
30 applies electrosurgical energy to the held particular tissue of the patient 11 in response to the application of the predetermined force for the sealing the particular tissue between the pair of end effectors 16.

The return electrode 24 is alternatively shown in Figure 1 on one of the pair of end effectors 16 opposite the active electrode 23. The return electrode 24 when
35 on the one of the pair of end effectors 16 that carries the active electrode has an electrical insulator is disposed between the active electrode and the return electrode shown in Figure 3. The return electrode is specifically a pad connected to the tissue

5 of the patient 11 in shown Figure 1.

The yielding member 19 can be a hydraulic coupling best shown in Figure 6 as part of the lost motion connection between 18 and is located between the pair of end effectors 16 at the patient end 14 and the actuator 15 at the user end 13. The hydraulic coupling is preferably located near the actuator 15 at the user end 13
10 but can be anywhere. The hydraulic coupling can include piston 31 attached to elongate transfer rod 21. Fluid is compressed and metered by valve 33 to a floating plug 34 which is loaded by a spring 35 thus the compressive nature of fluid is primarily used to add the resilient bias.

The yielding member 19 could alternatively be a slip clutch 36 within the lost
15 motion connection 18 located between the pair of end effectors 16 at the patient end 14 and the actuator 15 at the user end 13 as shown in Figure 7. The slip clutch 36 is most preferably located near the actuator 15 at the user end but could be elsewhere.

The slip clutch 36 in Figure 7 is connected to elongate transfer rod 21 and
20 includes a wheel 37 journalled to rotated when the rod 21 reciprocates. There is a brake band 38 pivotally mounted at 39 to be rotated against the wheel 37. The function connection between the wheel 37 and the brake band 38 acts as the yielding member 19 in this slip clutch 36. Although a spring 40 is shown the yielding is primarily the friction load of the brake.

25 The pair of end effectors 16 have opposing faces each of an equal and preset area. The opposing faces clamp the particular tissue of the patient 11 therebetween as seen in Figure 1 with the force from the yielding member 19 so that a preferred pressure is applied to the particular tissue.

A method allows a user to clamp and apply force and electrosurgical energy
30 to seal and/or join particular vascular tissue of a patient 11 with the clamping force mechanism 10 of the instrument hereinbefore described. The steps of the method including transferring user manipulation of the actuator 15 to the pair of end effectors 16 with the lost motion connection 18, maintaining a predetermined clamping force application during sealing and/or joining the particular tissue of the
35 patient 11 between the pair of end effectors 16 with the lost motion connection 18 and applying electrosurgical energy for sealing and/or joining the held particular tissue of the patient 11 in response to the clamping thereof between the pair of end

5 effectors 16 with the control associated with the electrosurgical energy supply 25.

The method step of applying electrosurgical energy includes responding to the parameter of the temperature of the particular tissue of the patient 11 between the pair of end effectors 16 during delivery of electrosurgical energy with the feedback circuit 26 including the temperature sensor 28 carried on one of the opposed faces
10 17.

The method step of applying electrosurgical energy includes responding to the impedance of the particular tissue of the patient 11 between the active electrode and return electrode during delivery of electrosurgical energy with the impedance monitor
27.

15 The method step of maintaining the predetermined clamping force application during sealing and/or joining of the particular tissue of the patient 11 by shifting of the yielding member 19 in the loss motion connection 18 with the actuator 15 so the opposing faces clamp the particular tissue of the patient 11 therebetween with force from the yielding member 19.

20 The method step of shifting with the actuator 15 secures the predetermined clamping force application during sealing of the particular tissue of the patient 11 by the resilient bias of the yielding member 19 and by including the step of urging with the spring 20.

The method step of shifting with the actuator 15 secures the predetermined
25 clamping force application during sealing of the particular tissue of the patient 11 by the yielding member 19 and by including the step of moving the pair of end effectors 16 between their open position for receiving the particular tissue of the patient 11 to the clamping position with the elongated transfer rod 21 located between the spring 20 near the actuator 15 and the pair of end effectors 16 at the patient end
30 14.

The method step of shifting with the actuator 15 secures the predetermined clamping force application during sealing of the particular tissue of the patient 11 by the resilient bias of the yielding member 19 and by including the step of urging with the hydraulic coupling as part thereof.

35 The method step of shifting with the actuator 15 secures the predetermined clamping force application during sealing of the particular tissue of the patient 11 by the resilient bias of the yielding member 19 and by including the step of urging with

5 the slip clutch 36 as part thereof.

The method step of maintaining the predetermined clamping force application during sealing of the particular tissue of the patient 11 and by the step of using the force from the yielding member 19 so that pressure is applied to the particular tissue.

5 What is claimed is:

1. A clamping force mechanism 10 for an instrument for allowing a user to clamp and apply force and electrosurgical energy to seal and/or join particular vascular tissue of a patient comprising:

an elongate support 12 having a user end 13 and a patient end 14;

10 an actuator 15 at the user end 13 for operation by the user;

a pair of the end effectors 16 at the patient end 14, at least one of the pair of end effectors 16 connected to the actuator 15 for operation thereby and from the user end 13 to control 30 the relative motion between the pair of end effectors 16, the pair of end effectors 16 each having an opposing face 17 of an area for
15 contact with the particular tissue of the patient;

a lost motion connection 18 between at least one of the pair of end effectors 16 at the patient end and the actuator 15 at the user end 13, the lost motion connection 18 for transferring user manipulation of the actuator 15 to at least one of the pair of end effectors 16 for maintaining a predetermined clamping force
20 over the face area during sealing of the particular tissue of the patient between the pair of end effectors 16;

an active electrode carried on one of the pair of end effectors 16;

a return electrode 24 in contact with the tissue of the patient for forming an electrosurgical circuit between the active and return electrodes 24,

25 an electrosurgical energy supply 25 connected across the active electrode of the pair of end effectors 16 and the return electrode 24, the electrosurgical energy supply 25 for delivery of electrosurgical energy through the electrosurgical circuit between and across the active electrode and the return electrode 24 when the particular tissue of the patient is held by the pair of end
30 effectors 16, and

a control 30 associated with the electrosurgical energy supply 25 for applying electrosurgical energy to the held particular tissue of the patient in response to the application of the predetermined force for sealing the particular tissue between the pair of end effectors 16.

35 2. The clamping force mechanism 10 of Claim 1 wherein the lost motion connection between the actuator 15 and the pair of end effectors 16 includes a yielding member 19, and the opposing faces 17 clamp the particular tissue of the

patient therebetween with the force from the yielding member 19 over the face area to achieve a predetermined force during clamping and while sealing.

3. The clamping force mechanism 10 of Claim 2 wherein a locking linkage 22 coupled to the actuator 15 and the yielding member 19 retains the opposing
5 faces 17 held against the particular tissue of the patient therebetween with the force from the yielding member 19 over the face area to achieve the predetermined force and stepped latching positions on the actuator 15 permit the user to selectively set the locking linkage 22 coupled therewith so the yielding member 19 establishes the selected force over the face area relative to particular vascular tissue sealed to retain
10 the predetermined force in accord with the particular tissue being sealed.

4. The clamping force mechanism 10 of Claim 1 wherein the electrosurgical energy supply 25 includes an electrosurgical generator 26 having a feedback circuit 27 in circuit with the active electrode and the return electrode 24, the feedback circuit 27 responsive to the parameters indicative of energy delivery
15 across the particular tissue of the patient interposed between the end effectors 16.

5. The clamping force mechanism 10 of Claim 5 wherein the feedback circuit 27 includes an impedance monitor 29, the impedance monitor 29 electrically hooked up to the electrosurgical generator 26, the impedance circuit responsive to the parameter of the impedance of the particular tissue of the patient between the
20 active electrode and return electrode 24 during delivery of electrosurgical energy.

6. The clamping force mechanism 10 of Claim 4 wherein the feedback circuit 27 includes a temperature sensor 28 carried on one of the pair of end effectors 16, the temperature sensor 28 is responsive to the parameter of temperature of the particular tissue of the patient between the pair of end effectors
25 16 during delivery of electrosurgical energy.

7. The clamping force mechanism 10 of Claim 1 wherein the yielding member 19 is a spring 20, as part of the lost motion connection 18 between the pair of end effectors 16 at the patient end 14.

8. The clamping force mechanism 10 of Claim 6 wherein the lost motion
30 connection 18 includes an elongated transfer rod 21 between the spring 20, near the actuator 15 and the pair of end effectors 16 at the patient end 14, the rod coupled to the pair of end effectors 16 for movement thereof between an open position for receiving the particular tissue of the patient to a clamping position for maintaining

the predetermined force on the particular tissue of the patient between the pair of the end effectors 16 and the return electrode 24 is on one of the pair of end effectors 16 opposite the active electrode.

9. The clamping force mechanism 10 of Claim 1 wherein the yielding
5 member 19 is a hydraulic coupling as part of the lost motion connection 18 between the pair of end effectors 16 at the patient end 14 and the actuator 15 at the user end 13, the hydraulic coupling located near the actuator 15 at the user end 13.

10. The clamping force mechanism 10 of Claim 1 wherein the yielding
10 member 19 is a slip clutch 36 within the lost motion connection 18 between the pair of end effectors 16 at the patient end 14 and the actuator 15 at the user end 13, the slip clutch 36 located near the actuator 15 at the user end 13.

11. The clamping force mechanism 10 of Claim 1 wherein the pair of end
effectors 16 have opposing faces 17 each of an equal and preset area, the actuator
15 applies a first force to grip the particular tissue of the patient therebetween and
15 the actuator 15 when advanced by the user applies a second greater force from the yielding member 19 so that pressure is applied to the particular tissue to clamp between the opposing faces 17 with a closure force in the range of 300 to 2500 grams.

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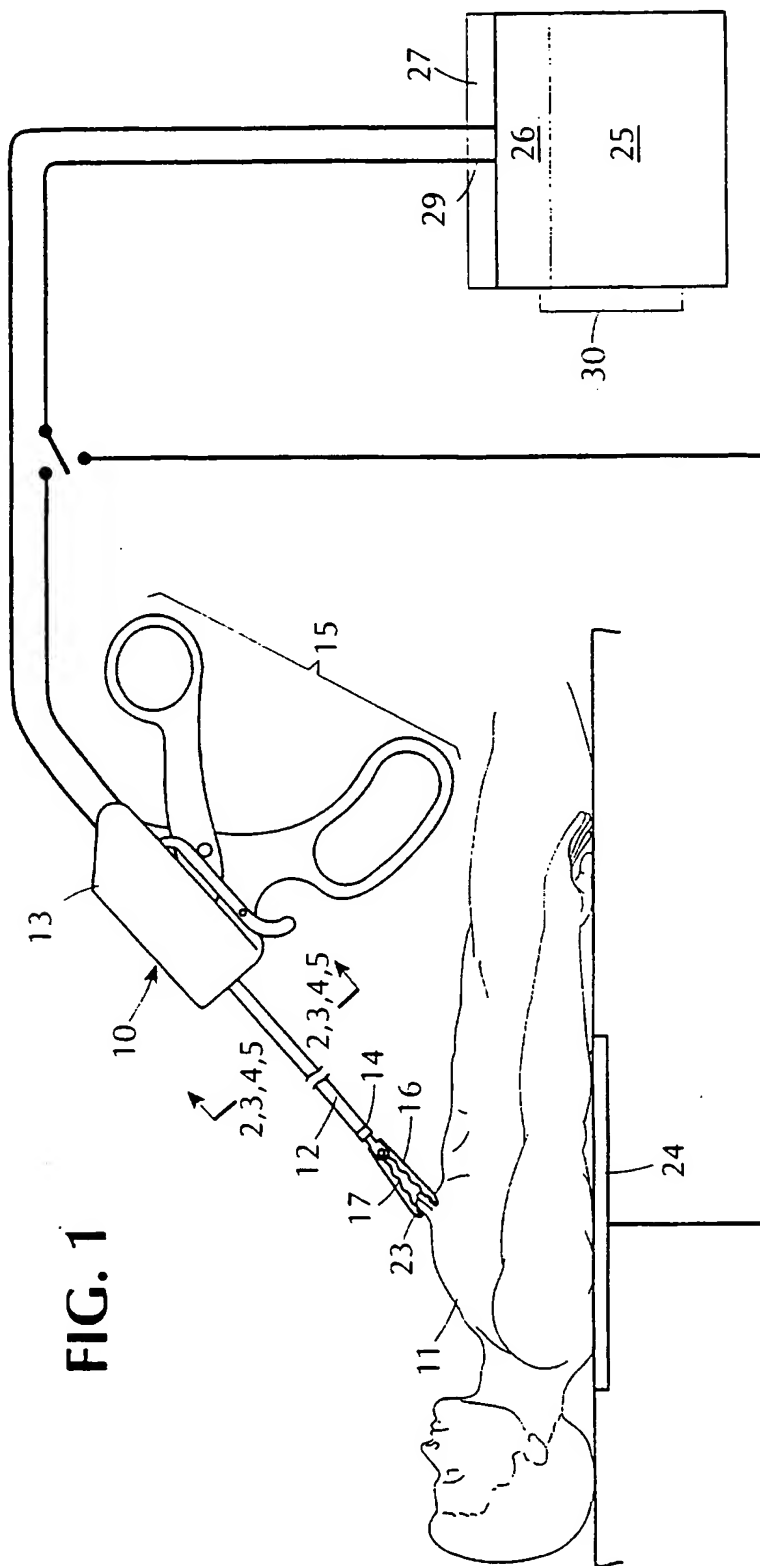
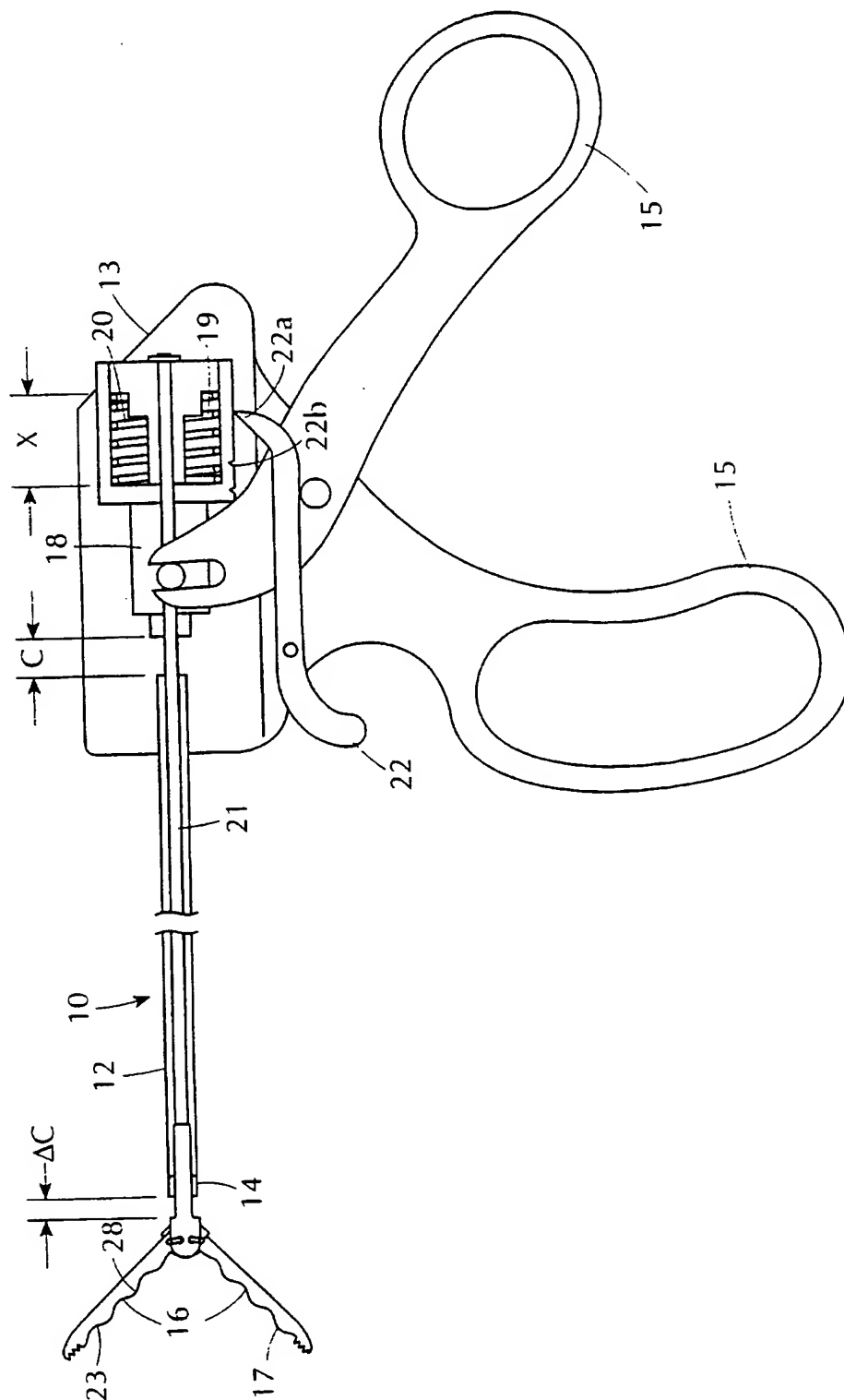
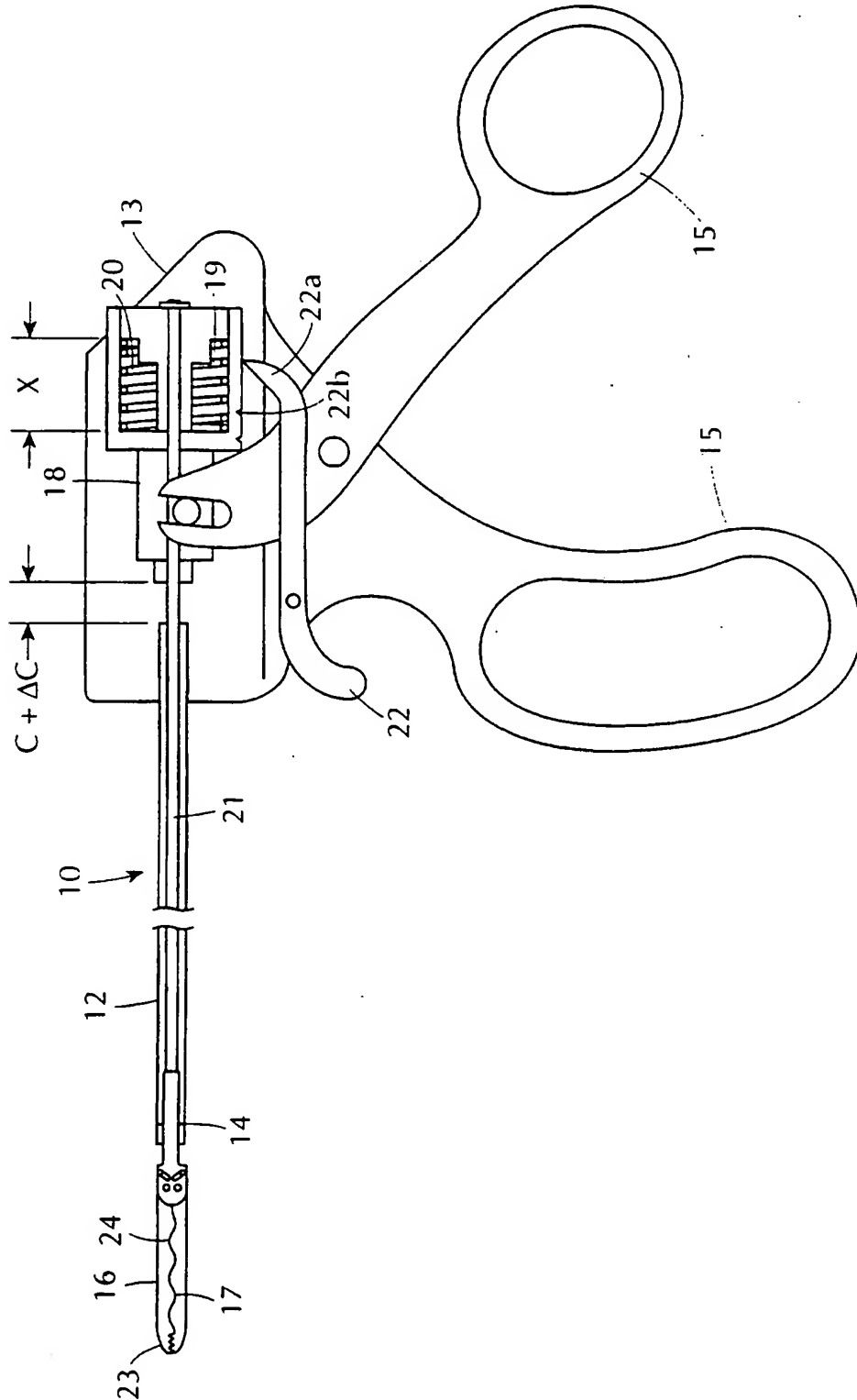


FIG. 2



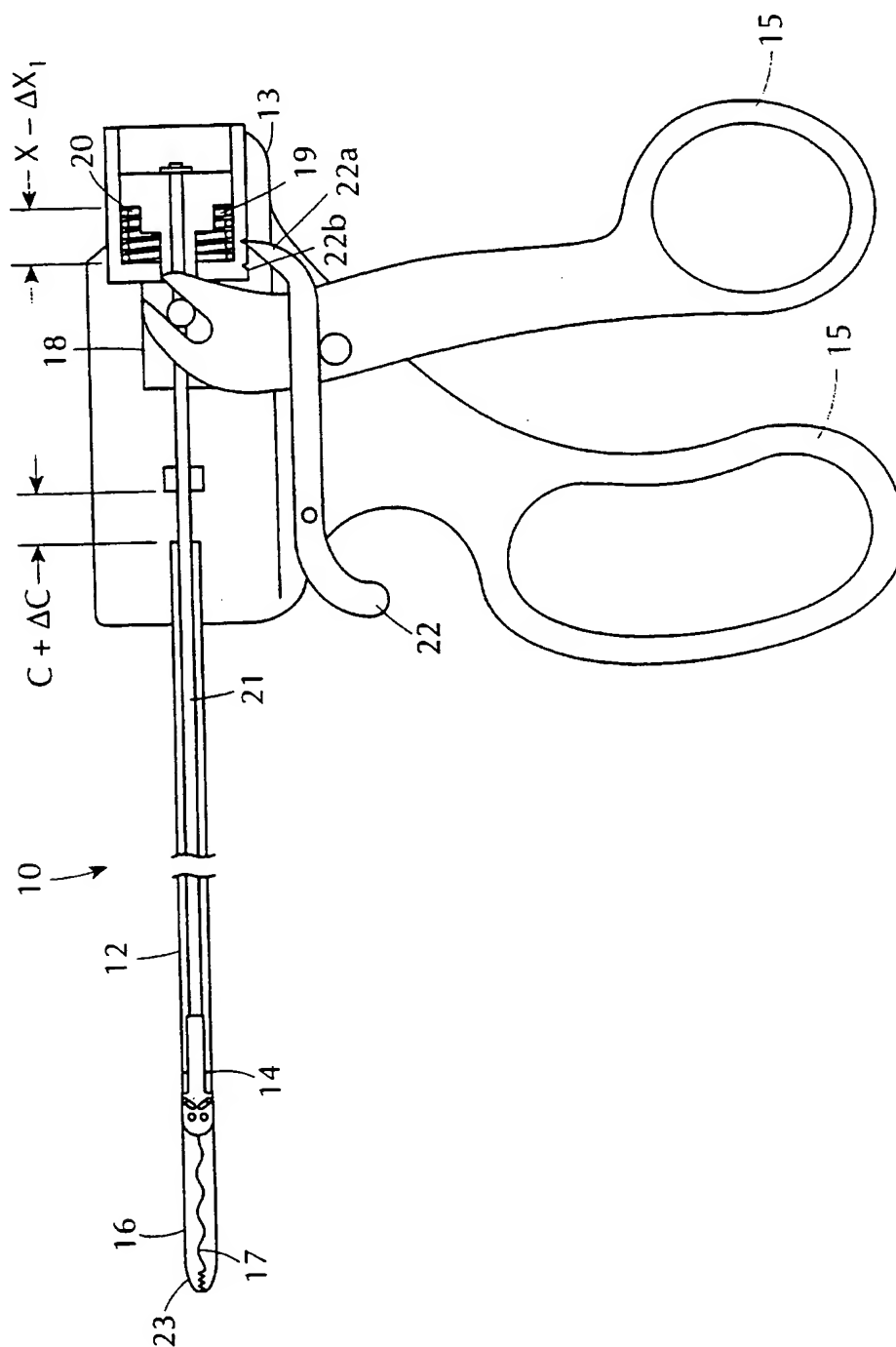
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FIG. 3



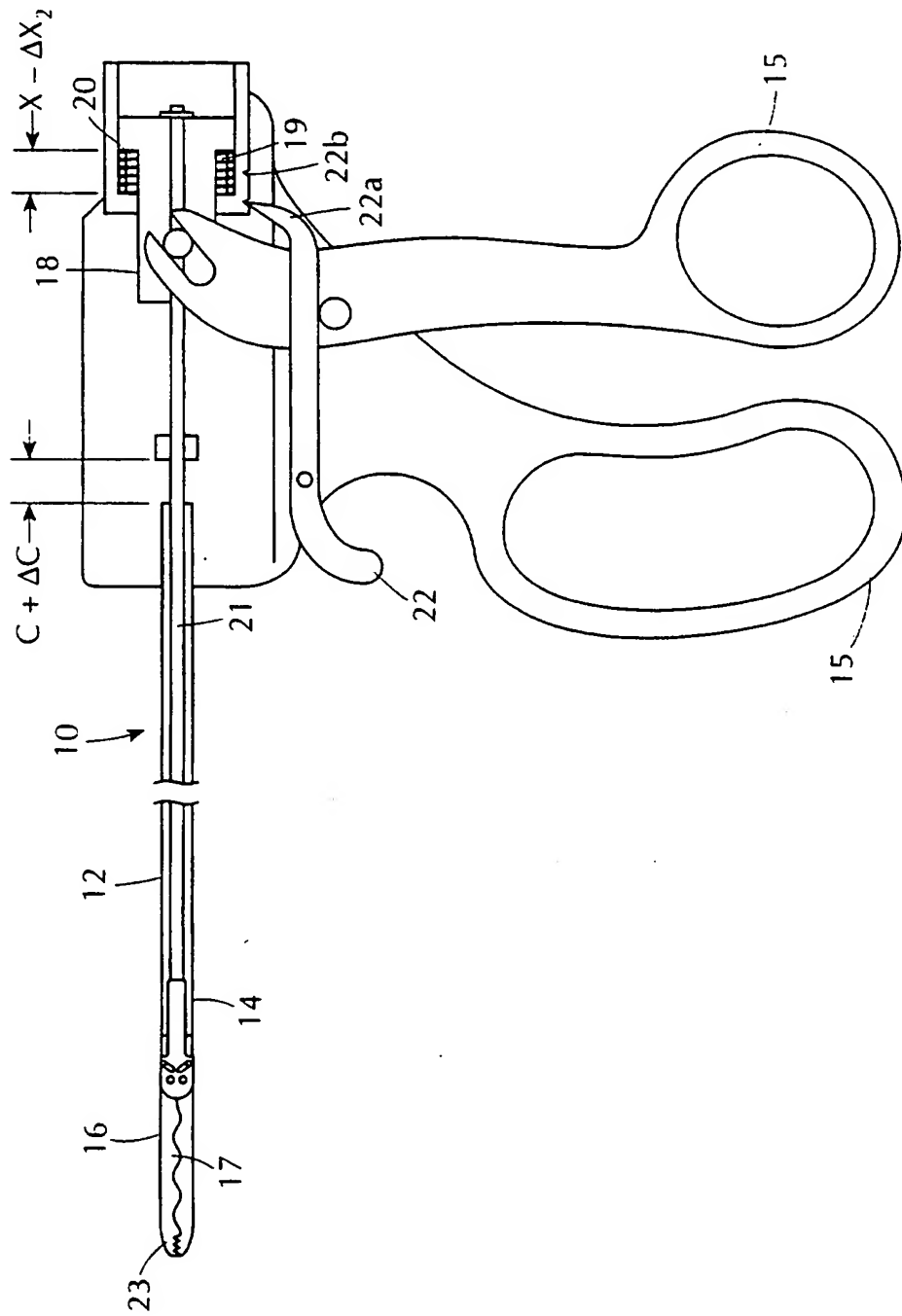
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FIG. 4



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FIG. 5



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FIG. 6

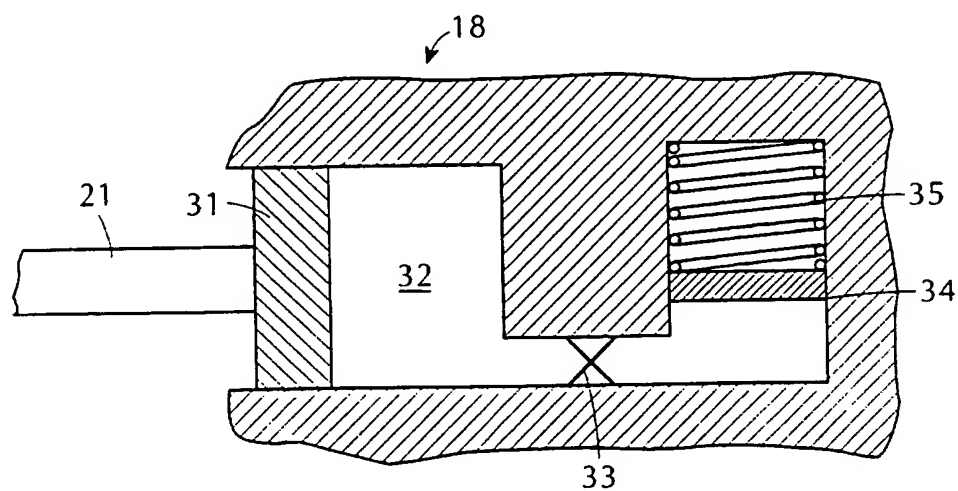
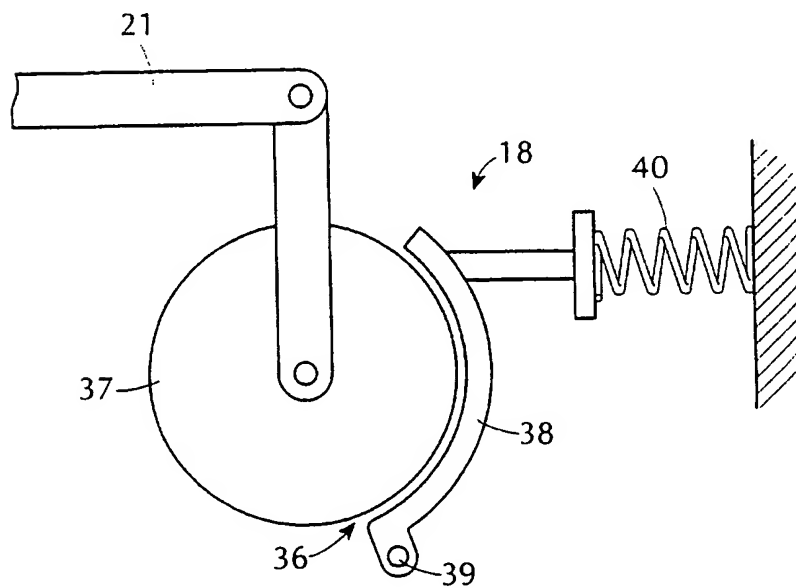


FIG. 7



INTERNATIONAL SEARCH REPORT

Inter national Application No
PCT/IB 96/00791

A. CLASSIFICATION OF SUBJECT MATTER
IPC 6 A61B17/39 A61B17/28

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
IPC 6 A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	WO,A,92 06642 (BOSTON SCIENTIFIC CORPORATION) 30 April 1992 see page 5, line 7 - line 10 see page 12, line 22 - line 30 ---	1
A	WO,A,95 07662 (MICROSURGE INC) 23 March 1995 see page 5, line 7 - line 24 -----	1

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Further documents are listed in the continuation of box C.

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Patent family members are listed in annex.

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Date of the actual completion of the international search

8 January 1997

Date of mailing of the international search report

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Gérard, B

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/IB 96/00791

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
WO-A-9206642	30-04-92	US-A- 5190541	02-03-93
		CA-A- 2094159	18-04-92
		EP-A- 0553242	04-08-93
		JP-T- 6502328	17-03-94

WO-A-9507662	23-03-95	DE-T- 4496959	26-09-96
		US-A- 5499998	19-03-96

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